



Radiographers' Journal



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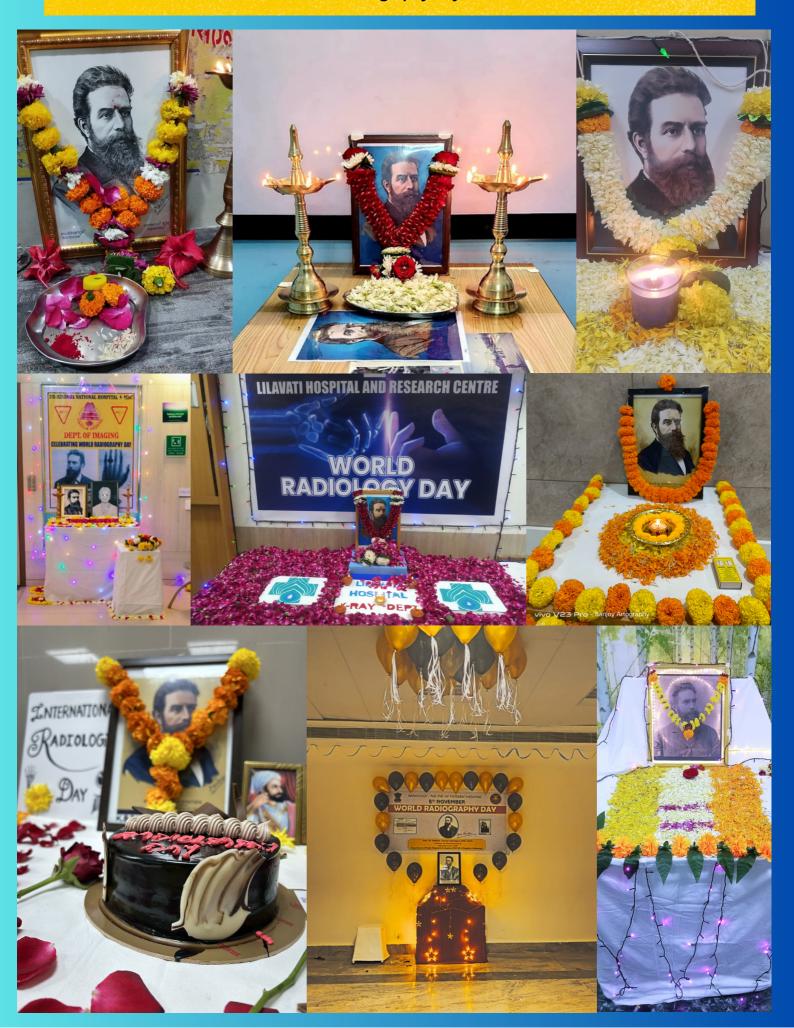
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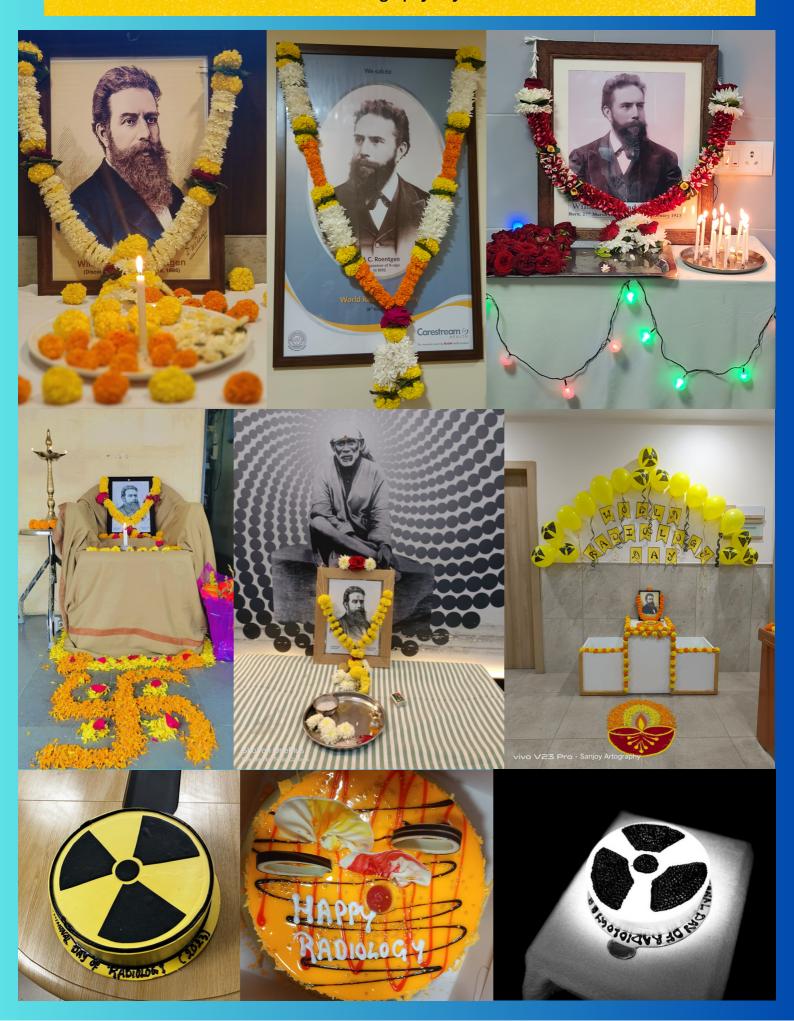
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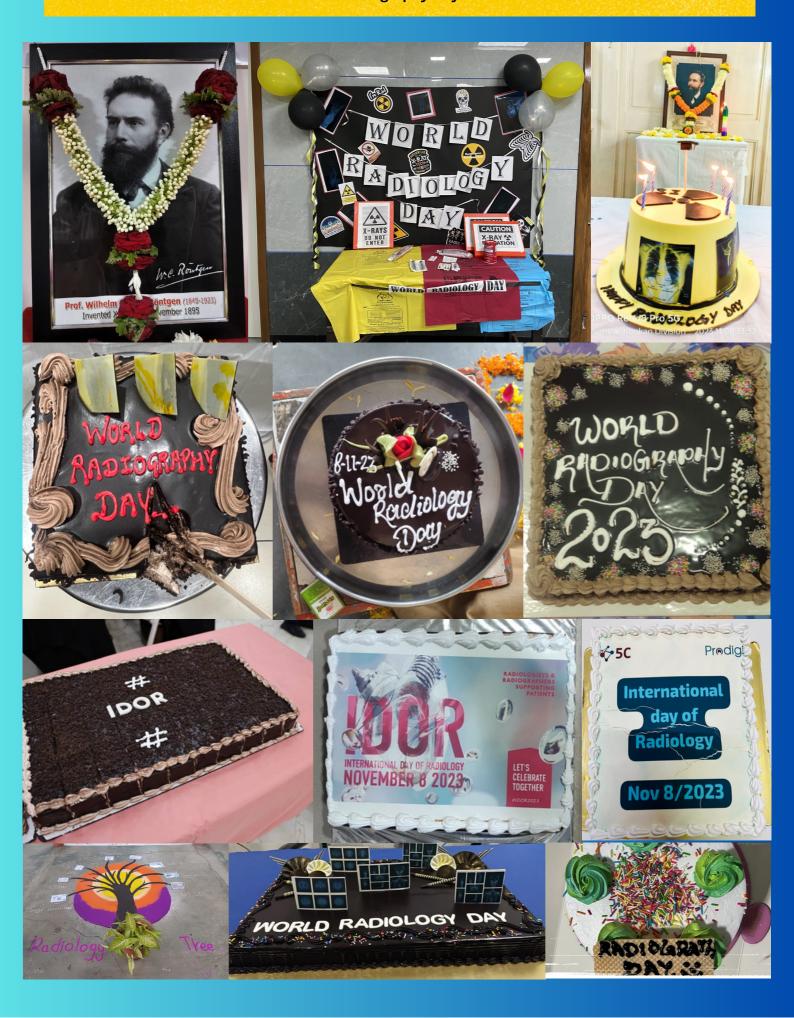
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Triple - Phase MDCT of Liver Scan protocol modification to obtain Optimal vascular and Lesion contrast

Divya Mary.S.D, Assistant Professor -BMIT, RR Institute of Medical Sciences- Bangalore

Introduction:

Hepatocellular carcinoma (HCC) is the fifth most common cancer in men and the eighth most common cancer in women. Currently, it is one of the most common .Causes of cancer related death worldwide. HCCs derive their blood supply predominantly from the hepatic arterial system, Whereas normal liver parenchyma receives 70-80% of its blood supply from the Portal vein. Dynamic contrast-enhanced imaging studies exploit this physiologic difference by Imaging the hepatic parenchyma and HCC during the arterial phase of contrast Enhancement, when differential enhancement maximized. With advances in helical computerized tomography (CT) with greater anatomic Coverage, more scanning times have revolutionized hepatic imaging. The entire Liver can be evaluated in a single breath-hold without respiratory miss-registration. Hepatic circulation has two major components: Arterial and portal venous. A rapidly injected contrast bolus can opacify the liver in two stages: an initial hepatic arterial phase followed by a portal venous phase. Consequently, optimizing the scan window has become critical. The mini-bolus and automated techniques have inherent drawbacks including limited

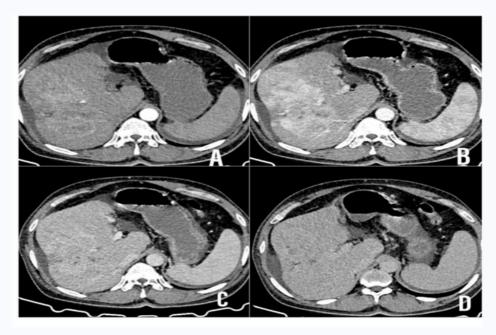
Availability, added cost of the automated-technique software, and increase in table time needed for review of mini-bolus images to calculate the time delay thereby patient throughput. decreasing Because of the reasons mentioned above, studies have been carried out using fixed timing delays for a variety of examinations, including hepatic imaging. A bolus-tracking technique has become widely available for the optimization of scan timing in individual patients to compensate for the variability of circulation time between patients. The purpose of our study was to optimize scan delays for

hepatic arterial and portal venous phases for bolus-tracking techniques in multi detector Computed tomography (MDCT) of the liver. With the advent of MDCT, the acquisition time for whole liver imaging is fewer than 5-10 seconds. Such a short acquisition time provides an opportunity to capture peak enhancement in visceral organs by optimizing contrast medium injection and scan protocols.

However, an off-timing scan markedly increases the risk of suboptimal contrast Enhancement. A bolus-tracking technique has become widely available and may be indispensable for the optimization of scan timing in individual patients to compensate for the variability of circulation time between patients. Multiphase CT improves the sensitivity of liver lesion detection .MRI, despite being recognized to be superior in characterizing focal liver lesions, remains a secondary tool due to limited resources in most centers in India.

Standard Parameters for Abdomen Triple Phase Study:

Scan Phase	Scan Delay	Pitch	Slice Thickness
Arterial phase	4 secs	1	5mm (recon-o.5 to 1mm)
Portal phase	19 secs	1	5mm(1mm)
Venous phase	44 secs	1	15mm (1mm)
Delayed phase	180 secs	1	5 mm (1mm)



Shows the different phases of triple phase study of Standard protocol.

A) Arterial phase ,B) Portal phase

C) Venous phase & D)Delayed phase

Contrast Material Injection:

All patients were administered non-ionic iodine contrast material containing 300 mg/mL (Omnipaque 300) using a pressure injector (MEDRAD salient) at a rate of 4.5-5 mL/s through a 18-gauge plastic IV catheter placed in an upper extremity vein, typically in an antecubital vein. The volume of contrast material delivered was 1.5 mL/kg of body weight in all patients.

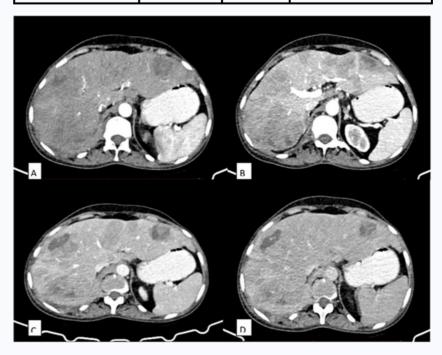
A Monitoring program was used to commence the diagnostic scans after contrast injection. This enabled real-time monitoring and the automatic calculation of CT values in a region of interest, and manual initiation of a diagnostic scan after the CT value reached a threshold. The region-of-interest cursor for bolus tracking was placed in the aorta at a level just above the diaphragmatic dome; this level was also used as a starting position for diagnostic scans. Real-time low-dose (120 kVp, 50 mA) serial monitoring scans were initiated 4 seconds after the start of contrast medium injection. During the 5-second interval between contrast injection start and the monitoring scan start, patients were carefully observed by a radiologist for extravasation or acute adverse events caused by the contrast medium injection.

Conclusion

The following conclusions can be drawn from this study: Using the bolus-tracking method, scan delays need to be optimized for portal venous and hepatic venous phases. A scan delay of 8 s, after trigger threshold (100 HU) is reached in the lower thoracic aorta, is optimal for the late arterial phase imaging. This phase is most helpful for assessment of hepatic arterial tree. The liver parenchyma showed a maximum enhancement at 48 s scan delay. This phase is optimal for assessment of hypovascular lesions like metastases from primary in the lung or colon.

Modified parameters for abdomen triple phase study

Scan Phase	Scan Delay	Pitch	Slice Thickness
Arterial phase	8 sec	1.2	5mm (recon-o.5 to 1mm)
Portal phase	23 sec	1.2	5mm (1mm)
Venous phase	48 sec	1.2	5mm (1mm)
Delayed phase	180sec	1.2	5mm (1mm)



Shows the different phases of triple phase study of Modified protocol .

A) Arterial Phase ,B)Portal phase,

C)Venous phase & D)Delayed phase

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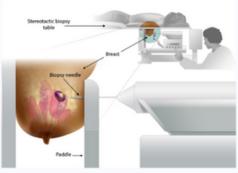
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Stereotactic Biopsy

Harshad P Naik, M.Sc. MIT, K.S. Hegde Medical Academy, Nitte Deemed to be University, Mangalore

The majority of mammographic detected questionable lesions are benign, and it is noticed that there is emerging interest among radiologist and patients in alternative to surgical biopsy for identifying these lesions. Stereotactic breast biopsy is an X-ray guided method for localising and quantifying breast lesions discovered on mammography, and considered to be suspicious for cancer. Its use in sampling small, non-palpable breast lesion using fine needle aspiration for cytology and, more recently, core needle biopsy for histology. Stereotactic biopsy have a sensitivity of 90-95 percent for cancer detection as compared to routine surgical breastbiopsy. Procedure is also quicker, cheaper and easier than standard practice of preoperative, mammographically guided localization followed by surgical biopsy. The first prone stereotactic table was acquired at the University of Chicago in US in 1986.It is used for non-palpable suspicious lesions identified on mammography or DBT but not visible on ultrasound.





Indications

- BI-RADS 5 (highly suggestive of malignancy)
- BI-RADS 4 (suspicious for malignancy) abnormalities.
- These include masses, architectural distortions, developing asymmetries and calcifications.
- Cancer Treatment planning, histological confirmation of BI-RADS 3 (Probably benign) lesions may be required in patients awaiting organ transplantation or women planning to become pregnant
- Absence of MRI-guided biopsy facility in a centre.
- Prior to breast conservation surgery for biopsy-proven impalpable lesions that require excision.

Contraindications

- Inability to visualize the target breast lesion at the time of biopsy is an absolute contraindication.
- Neuromuscular disorders such as Parkinson's disease may limit the capacity of the patient to lie still.
- Overweight patients, as most prone tables have a weight limit between 136 and 158 kg.
- Bleeding or clotting disorder

Stereotactic equipment

Can be carried out in 2 ways:

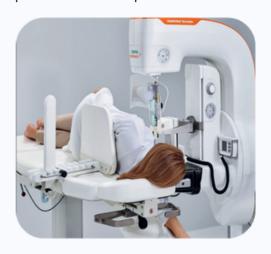
- A dedicated prone table with the patient lying prone
- Upright mammographic add-on system with the patient in a sitting or lateral decubitus position. An add-on stereotactic localization device can be fitted on the mammography machine prior to the biopsy which converts a standard mammography machine into a stereotactic biopsy unit. As the same machine is used for both mammography as well as biopsy, lesion visualization at the time of biopsy is good, as the resolution and quality of the image remains the same.





Patient carrier

The patient needs to be comfortable during the procedure as procedure may take up to 15-30 min avoid movement-related and to complications. Dedicated stereotactic biopsy chairs are available which allow biopsies in the sitting up and decubitus positions. However. up the patient propping supporting the back and arms is vital. If a prone table is being used, the should patient be comfortably positioned and good padding provided where required





Computer

This is the brain of the procedure which uses the concept of Stereotaxis and calculates the depth of the lesion. A 'scout' image is acquired at an angle of 0°.A +15° image and a −15° image (the stereo pair) are acquired next. The lesion shows an apparent movement between these projections referred to as 'parallax shift' and is calculated relative to the reference point. Basic trigonometry is applied to determine the X-, Y- and Z-axis of the lesion to be biopsied. This is calculated by a computer software using information from the markings done by the operator on the computer screen and mimics depth perception performed by the human brain

Biopsy equipment

Core Biopsy (CB) or Vacuum Assisted Breast Biopsy (VABB) can be performed.

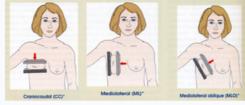
CB is equivalent to that of open surgical biopsies and is highly reproducible and reliable



VABB is directional and can acquire tissues up to 5 mm away from its own position, into the sampling chamber and cut it away from the surrounding tissue using vacuum action, compensating for subtle patient movements

Planning

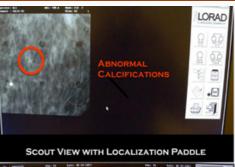
- CC, ML, LM or oblique views of breast can be used for the procedure.
- The biopsy approach could be vertical or lateral.
- The breast size, breast thickness upon compression, as well as the location of the lesion influence the approach.



Procedure

- Position the pt. in such a way that that the target is at center of the compression paddle, confirmed by taking the 0°scout view.
- Stereo pair images are obtained by moving the X-ray tube and detector assembly +15° and −15° relative to the 0° position on the scout image
- The operator marks the center of the lesion on both stereo images on the monitor.
- The X, Y and Z co-ordinates of the lesion are calculated by the computer
- The operator cleans the skin and injects 2% lignocaine (for CB) ± epinephrine (For VABB)
- A 2 mm skin incision is made for a CB, the needle is inserted and prefire and post-fire check images are taken to confirm optimum needle position
- For VABB, a 4 mm incision is made and firing may not be required and hence, a single set of check images may be acquired6-12 samples are obtained















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Recent Advancements in Pre-Patient Filters in Spectral Shaping Computed Tomography to Reduce the Radiation Dose

Abhijith S, M.Sc. MIT, K.S. Hegde Medical Academy, Nitte Deemed to be University, Mangalore

Introduction

Computed tomography(CT) is the most accurate and rapid diagnostic tool for most pathologic conditions. With the recent advancements in helical multi-detector CT, achieving the most accurate diagnostic information with minimum scan time is possible. Since CT uses ionizing radiation to obtain the image, it is important to reduce the radiation dose as possible for patients. There various dose reduction are techniques in CT, one such technique is pre-patient radiation filtration. In this article, recent advancements in pre-patient filtrations are discussed.

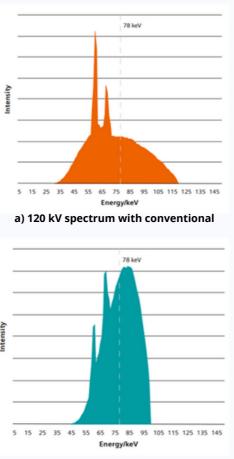
CT filter

Since the X-Ray beam used is polychromatic, filtering out the lowenergy photons is very important to reduce the patient dose. Widely used filter materials are Al (aluminum), and Cu(copper) to filter out the low-energy photons. compared conventional X-Ray, CT possesses problem called beam another hardening artefact. This means the mean energy of the X-Ray spectrum increases as it passes through the object. This is avoided by using a bow tie filter. This is the basic type of filter used mostly in all CT scanners. In addition, there is also a theory that materials between the atomic numbers 40 to 83 provide adequate filtration for the diagnostic range. The materials that reach the requirement for filter material and adequate filtration are Sn(tin) and Au(gold).

Tin filtration (k-edge)

There will be an abrupt increase in characteristic absorption of the radiation just above the K-edge of the filter material. Tin (Sn) has an atomic number of 50 and its K-edge is 29.2 keV. The k-alpha and k-beta of the target tungsten are approximately 60 and 70 keV respectively. Tin filter eliminates the photons at a range of 30 – 40 keV causing significantly

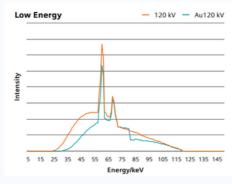
increased filtration and also reduced noise as compared to conventional filters used. The mean energy of the spectrum increases thereby reducing the beam hardening artefact. The use of this with traditional filters reduces the patient dose maintaining the image quality at the diagnostic range.



b) 100 kV spectrum with tin+convetional

Gold as a filter:

The atomic number of gold is 79 and the K-edge is 80.72 keV. This abruptly filters the photons at just above its K-edge, which means approximately at

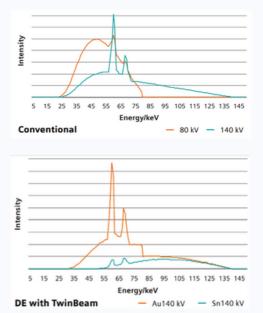


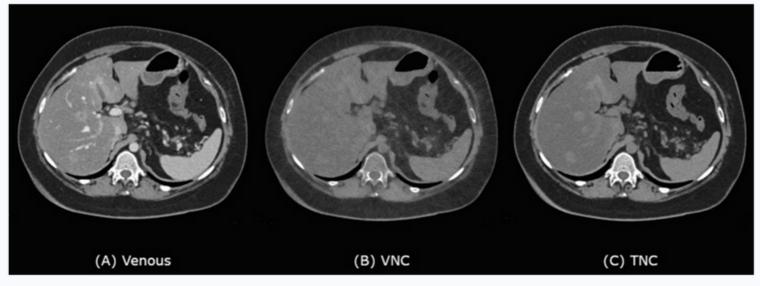
120 kV spectrum (conventional filter) with and without gold filter

and above 81 keV. This filtration decreases the mean energy of the spectrum. This also provides a good-quality image with a significantly lower patient dose.

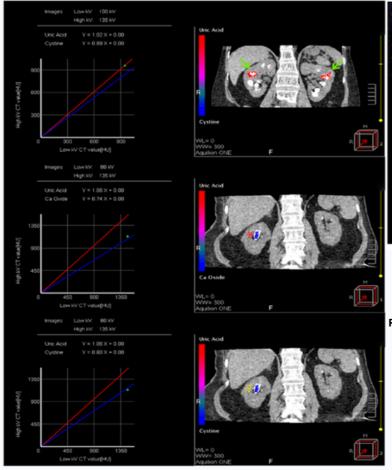
Spectral CT imaging

This is imaging of the object with two different energy spectra of X-ray. This helps in the decomposition of the material by their different X-ray absorption property at different energy levels. This is the most recent advancement in CT where this is achieved in many ways by various vendors. By Siemens Healthneers this is achieved by using two different Kedge filters at each source in a dualsource CT scanner. Above mentioned two filters, where the tin (Sn)filter increases the mean energy of the spectrum by filtering the low energy photons above its K-edge (29.2keV) and Gold (Au) decreases the mean energy of the spectrum by filtering the photons above its K-edge (80.72 keV). These two combinations give two different spectra with different mean energy. This makes it possible to image the object on a dual-energy basis. Currently applied in various applications such as metal artefact reduction, virtual non-contrast imaging, urinary stone classification etc.





Virtual non contrast image generated by DECT with true noncontrast CT image



Urinary calculi characterisation





Sn 140 kV C-spine CT with lesser radiation dose and reduced metal artefact

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आप भी अपना पाठक धर्म निभाएँ

पत्रिका का अंक मिला, डाउन लोड किया, पढा और डिलीट कर दिया. केवल इससे पाठक धर्म नहीं निभ जाता. पत्रिका में प्रकाशित सामग्री से आप सहमत हो सकते हैं या उसमें आप कुछ और जोड़ सकते हैं, तो ऐसे मामलों में अपनी टिप्पणी अथवा प्रतिक्रिया हमें अवश्य लिख भेंजे. इसी प्रकार पत्रिका में जो मुद्दे उठाए गए हों, जो प्रश्न खड़े किए गए हों, उन पर भी खुल कर बहस करें और हमें लिख भेंजे. तात्पर्य यह है कि आप केवल पाठक ही न बने रहें, पाठक धर्म भी साथ में निभाते रहें इससे जहां अन्य पाठक बंधू लाभान्वित होंगे वहीं हमें भी विभिन्न रूपों से मार्गदर्शन मिलेगा. हाँ तो, जब भी समय की मांग हो, कलम उठाना न भुलें.

और एक बात, ये अंक हमने आप तक पहुंचाया, एक प्रबुद्ध रेडियोग्राफर के नाते अब ये आप की ज़िम्मेदारी बनती है कि इस अंक को आप भी और रडीओग्राफेर्स तक पहुंचाए यानि फॉरवर्ड करें.

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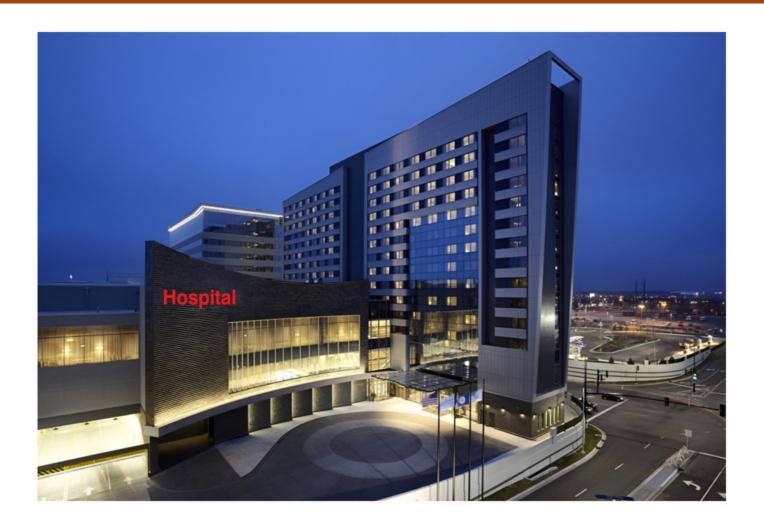
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Bolus

Anupama. L, Tutor -Radiotherapy Technology, RR Institute of Medical Sciences- Bangalore

Introduction:

It is a tissue-equivalent material (material which has the property equivalent to the tissue). Bolus in radiotherapy means a soft material placed over the body.

About it:

To treat lesions on or close to the skin surface, bolus material can be placed over the skin region undergoing RT to increase radiation dosage at the skin surface. The bolus material can be a soft, rubbery tissue equivalent material placed in direct contact with the patient's skin surface.

Bolus is used to either increase the surface dose or to reduce unwanted deep penetration. Sometimes bolus is only used when there is a risk of microscopic residual disease on the skin. It is usually used to ensure 100% dose at the surface.

Bolus should always extend beyond the field edge so as to avoid a sharp gradient and variation in bolus thickness should be gradual.

It is also used to modify the treatment depth if limited range of electron energy is available. Based on the energy of the photon used the thickness of the bolus material varies.

The bolus material increases the radiation dosage to the patient by providing scattering of the beam and build-up of the radiation dose prior to the beam's entry into the skin. As a result, the radiation beam deposits the maximum radiation dosage at or near the skin surface, rather than penetrating the skin and delivering the maximum dosage several cm's below the skin surface, as the radiation beam would normally do.

There are different types of bolus:

MaterialTrade NameGelsSuper flabMoldable bolusesSuper stuff, AquaplastWaxesParaffin wax



Thermoplastic mask (H&N) with bolus



Thermoplastic mask with bolus during CT simulation



Chest wall irradiation with bolus



1cm superflab bolus

Conclusion:

PROS: Desired amount of dose can be achieved in the surface area. CONS: Skin sparing effect cannot be achieved resulting in poor cosmesis. It will increase the skin reaction significantly.

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Thanks in advance,

Editor

International Radiography Day Celebrations at IIT Bombay Hospital, Powai, Mumbai









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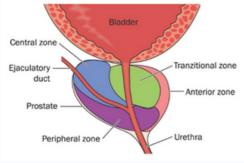


The value of diagnostic imaging in Benign Prostatic Hyperplasia.

Tancia Pires, M.Sc. MIT, K.S. Hegde Medical Academy, Nitte Deemed to be University, Mangalore

Introduction

Prostate, the walnut shaped organ is a part of the male reproductive system and is involved in the formation of alkaline semen that carries the male gamete. Enlargement of this organ or Benign Prostatic Hyperplasia (BPH) has been one of the most frequent diagnoses leading to urology referral. The growth of BPH likely begins before a man reaches age 30, with approximately 8% of men having histologic evidence of BPH by 40 years of age. Nearly 80% of men develop BPH, and as many as 30% receive treatment for this condition during their lifetime. Thus, the burden of BPH on the health care system, with respect to monetary expenditure and resource use, is substantial.



Zonal anatomy of the Prostate Gland. Courtesy:

https://atlanticurologyclinics.com/conditions/prostatitis-infection-of-the-prostate/

Symptomology

Along with the enlargement in the size of the prostate greater than 25 ml, decrease in the urinary flow rateis commonly seen due to impingement of the urethra that runs through the gland. These patients also demonstrate a high postvoid residual volume. The risk of acute urinary retention is also seen.

Severe complications of BPH include urinary retention, hydronephrosis, hydroureter, recurrent urinary tract infections, bladder calculi, recurrent gross hematuria, and ultimately, renal insufficiency. However, these are rare and occur only in severe enlargement. These data suggest that prostate size may be a factor in determining which patients with BPH

will develop what kind of complications. Hence measuring the volume through imaging and correlating with clinical symptoms becomes an essential aspect in treating BPH effectively.

Imaging Modalities aiding in diagnosis

1. Plain X-ray

radiographs Plain have limited prostate evaluation utility but are rarely used as a skeletal survey to assess follow metastases. However, traditionally, performing IVU was considered useful prior to initiation of the treatment for BPH. Potential benefits of upper urinary tract imaging with IVU in these patients include: determination of the presence and degree of upper tract obstruction urinary (hydronephrosis); estimation of renal function; evaluation of the bladder and prostate; detection of incidental upper tract (renal or ureteral) malignancies or stones; and medicolegal safety.

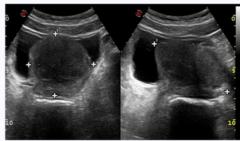
2. CT Scan

CT scan is not typically done for diagnosis, but BPH is identified when the prostate extends above the pubic symphysis on axial imaging. BPH can also be diagnosed on a CT scan with a volume greater than 30 ml (measured with the help of coronal reformate images).When compared with ultrasound and MR imaging, CT has a limited ability to define intraprostatic zonal anatomy although CT can define the relationships between the prostate and other pelvic organs, its in the diagnosis management of patients with BPH is limited.

3. Ultrasound

Ultrasonography of the prostate can be performed via a transabdominal, transrectal, or transurethral approach. Among these techniques, the transrectal approach is preferred by most physicians. Transurethral approach isn't utilized due to its

Prostate invasiveness. length measured in the sagittal plane, width and height are measured in the transverse plane. Prostate volume is then given by the formula: length × width \times height \times $\pi/6$. The average normal measurements are 3.75 to 4.00×2.5 to 3.00×3.1 to 3.8 cm (width x height x length) with a volume of 20 to 25 ml. Viewing the prostate in than two dimensions more important diagnostically because it greatly facilitates precise localization of a suspicious area for biopsy. The normal prostate of the young adult male is composed of homogeneous, low-level echoes, with the central and peripheral zone showing uniformly hyperechoic appearance. In men with BPH, the central gland typically appears hypoechoic when as compared with the peripheral portions of the gland, and as BPH develops, the peripheral gland becomes compressed and distorted and hyperplasia may be identified as a single, focal nodule or as multiple nodules within the transition zone.



Prostatic Volume measurement on USG.

Courtesv:

https://radiopaedia.org/cases/34645/studies/36 045?lang=us

4. MRI

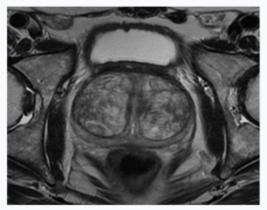
More than any other imaging modality, MR imaging accurately depicts internal prostatic zonal anatomy and displays the physiologic complexity of the gland.

Besides diagnosing BPH, MRI plays an important role in identifying carcinoma when a patient with BPH has increased PSA and suspicious or at high risk for developing prostate cancer. However, the presence of benign prostatic hyperplasia (BPH)

within the Transitional Zone of the prostate, can often mask or mimic malignancy. Hence multi-parametric MRI imaging proves to be essential for the correct diagnosis. This includes, routine T2 Weighted imaging (T2W), Diffusion studies (DWI) and Dynamic Contrast Enhanced (DCE) Examinations.

On T2Wimaging, using anatomic characteristics such as shape, structure, and growth pattern have given accurate differential diagnosis. Features such as homogeneous hypo intensity on T2W imaging, ill-defined margins, and lenticular shape have been shown to be specific for TZ cancers. Furthermore, the most recent PI-RADS classification has defined T2W imaging as the dominant pulse sequence for identifying TZ cancers.

It has been shown that DWI in addition to T2W imaging can improve cancer detection in the TZ across readers with varying expertise, However, other researchers opined that DWI has no additional value while using lower b values. More research in this would be required to



Axial T2W image showing enlarged transition zone with heterogeneous signal intensity.

Courtesy: https://radiopaedia.org/articles/benign-prostatic-hyperplasia

comment upon this controversy. A similar contradictory scenario has been identified in case of DCE- MRI in the differentiation of BPH and Prostatic Malignancy as the enhancement patterns in some variants of BPH are similar to those seen in malignant lesions.

5. Newer Trends in MRI

New technologic developments, such as the endorectal coil and 3D H-1 MR spectroscopic imaging of the prostate, are currently being tested in patients with prostatic disease. The endorectal coil provides more detailed anatomic information than the body coil and allows for better visualization of the neurovascular bundle. Such technology may lead to improved local staging of patients with prostate cancer. MR spectroscopic imaging of the prostate may allow for the detection of biochemical differences between BPH and prostate cancer where significantly higher choline levels and significantly lower citrate levels are observed in regions of cancer when compared with normal peripheral zone and BPH.

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रेडियोग्राफर को पढ़ाने ट्यूटर, लेक्चरर जैसी पोस्ट भी हो

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जर्मन वैज्ञानिक विलहेल्म कोनार्ड रोंजन ने 8 नवंबर 1895 को एक्स-रे का आविष्कार किया था। इसी उपलक्ष्य में हर वर्ष 8 नवंबर को विश्व रेडियोग्राफी दिवस मनाया जाता है। इस अवसर पर शासकीय कैंसर हॉस्पिटल में एक परिचर्चा आयोजित की गईं, जिसका शुभारंभ अस्पताल अधीक्षक डॉ. रमेश आर्य ने किया। उन्होंने कहा-रेडियोलॉजी ब्रांच चिकित्सा जगत की सबसे महत्वपूर्ण ब्रांच है। डॉ. प्रीति जैन ने कहा- पहले मेमोग्राफी, महिलाओं के एक्स-रे करने में मुश्किल आती थी, लेकिन अब नहीं। डॉ. ओपी गुर्जर, एमआरआई टेक्नोलॉजिस्ट गोकरण चतुर्वेदी, मानसिंग चौधरी, विनोद तिवारी, शरद जैन आदि का स्वागत किया गया। एमवायएच के रेडियोग्राफर अजय सोनी ने कहा- रेडियोग्राफर को पढ़ाने के लिए ट्यूटर, लेक्चरर जैसी पोस्ट निर्मित होना चाहिए।

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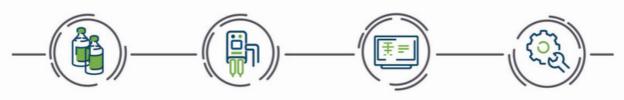
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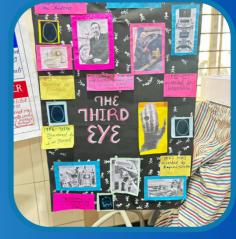
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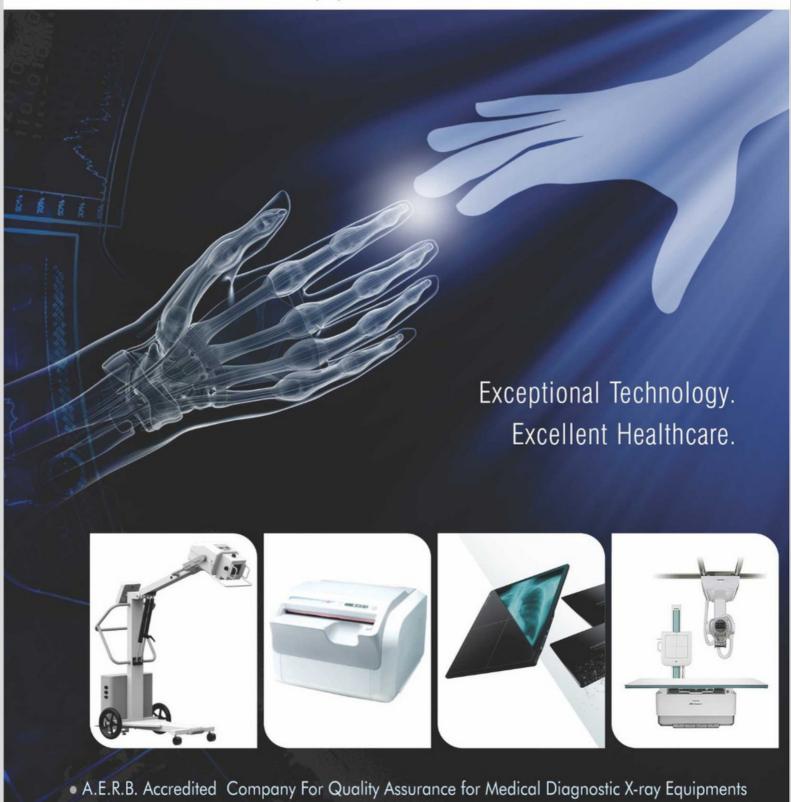


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Zero TE MRI

Apurva Dessai, M.Sc. MIT, K.S. Hegde Medical Academy, Nitte Deemed to be University, Mangalore

Introduction

Many people undergo CT examinations per year for many reasons. CT remains the first modality for many indications, such as acute cortical screening and bone assessment, especially for children. As we know, radiation exposure has many adverse effects and has always remained a great concern. These effects are primarily seen in children due to the increased sensitivity of the developing tissues or organs etc.(1)

Solid bone structures are challenging to see in MRI due to low proton density and short signal lifetimes. Conventional gradient echo or spin echo pulse sequences with echo times (TE) in the millisecond range are generally too slow for meaningful bone signal detection.(2)To overcome this problem, a new technique called zero TE is introduced in the MRI. Zero TE MR imaging is a novel technique achieves near-zero-time that а interval radiofrequency between excitation and data acquisition, enabling visualization of short-T2 materials such as cortical bone, meninges, tendons, etc.(1,3)

This ZTE sequence is applied at the readout period soon after applying the RF pulse. It is a sequence that gives a high-resolution image, and also, it is fast, silent and avoids the artifacts which occur due to the patient's movement. This technique is used in craniofacial, temporal bone, jaw, and spine because of its ultrashot TE. Image acquisition in ZTE needs high-performance coils with rapid transmit/ receive switching capabilities and make use of centerout K-space encoding.(1–3)

It can also be used in lung imaging; it is very difficult to image the lung by using MRI as there is a presence of the lung and cardiac motion. To avoid motion artifacts, image data are acquired at a defined phase of the respiratory cycle, typically in the end-expiratory phase.(4)

Image acquisition

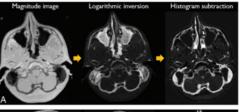
The readout gradient is switched during the RF pulse application, precluding slab selection. For the acquisition of high-bandwidth excitation with a short-duration hard pulse, ensure that the excitation is equally distributed and as consistent as possible across the entire FOV from the application of the excitation continuously.(1,2,5)The pulse is immediately followed by the 3D data acquisition. This uses the gradients, which are continuously modulated between repetitions, to sample the data along the radial trajectories in k-space instead of quickly turning it on and off.(1)

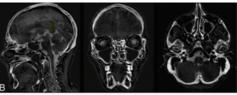
As there is a reduction in mechanical vibration, it reduces the noise. But for the radial filling technique, a greater number of TRs are required as compared to the 3D cartesian filling. But the scan time is reduced by applying short TRs and small flip quasi-steady-state angles for magnetization. A major part of the scan time is used in data acquisition, and less time is kept between the RF pulse and a single gradient step. (1,3)This helps in isotropic scanning avoiding the artifacts caused by the motion. Low flip angles and scanner safety measures counter the RF pulse duration, increasing the concern related to high SAR values. (1)

Image post processing

Raw images show signal void compared to the surrounding soft tissues, known as the "black-bone display." To improve the bone-air differentiation and generate a "bright bone display," which appears similar to the CT images. The black-bone also called magnitude images, signal intensity images, undergo correction section by section and normalize the mean soft-tissue signal within each section. Multiresolution ROI-based intensity correction was then applied to account for residual signal intensity variations and thus reduce overall image noise.(1,3)

Logarithmic inversion of the intensity-corrected data yielded preliminary bright-bone images without optimal bone-air delineation. An intensity histogram was generated, and an intensity mask was selected to remove the peak signal of air, generating the final pseudo-CT image and enabling the generation of 3D volume renderings at a separate workstation. (1,2)





ZTE image display. A- raw magnitude black-bone images underwent signal intensity correction on a section-by-section basis with normalization to mean soft-tissue signal. Multi-resolution ROI-based correction was then applied to account for residual signal intensity variations. Logarithmic inversion of the intensity-corrected data yielded bright bone images. Histogram subtraction was used to identify and mask the peak signal of air, thus generating the final pseudo-CT image. B- sample sagittal, coronal, and axial reformats of pseudo-CT reconstruction.

Discussion

Using the ZTE sequence made it easy to perform bone imaging in small clinical case series and ex-vivo studies of the cranial vault, face, jaw, and spine. The MRI provides superior softtissue detail and combination with ZTE bone sequence, gives a highly efficient and radiation-free evaluation in many pediatric neuroimaging, head/neck imaging, and musculoskeletal imaging. (1) It is proven that skull properties extracted from ZTE images were equivalent to those obtained on CT (5) Inversion recovery techniques can also yield T1-weighted ZTE images useful for assessing brain and spinal cord myelination, tumor and pituitary imaging, vessels, and airway.

Physician awareness, scanner and hardware compatibility, vendor sequence availability, clinical workflow, and image postprocessing and analysis are the limitations of using the ZTE sequence. (1) The method might also be of interest for musculoskeletal applications and the detection of traumatic injuries. (2). The other use of the ZTE sequence for PET/MR imaging would be lung visualization to improve the estimation of parenchyma attenuation and the detection of local coils. (3) The skull features conventionally estimated from CT images were accurately replicated with ZTE MR images. (5)

Conclusion

ZTE is a technique that provides radiation-free imaging with rapid, high-resolution, silent, and artifact-resistant properties equivalent to CT images. It can be combined with PET/MR imaging to appropriately depict lung morphology, which is of key importance for oncology applications.

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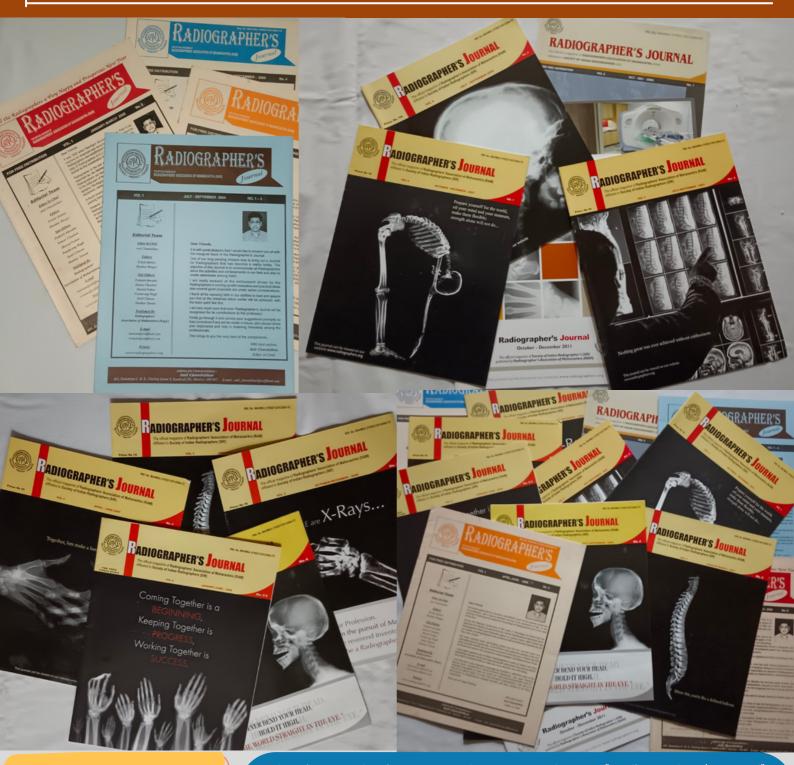
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